



Gold nanowires as future low power sensors

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Nanotechnology Group

27th October 2011



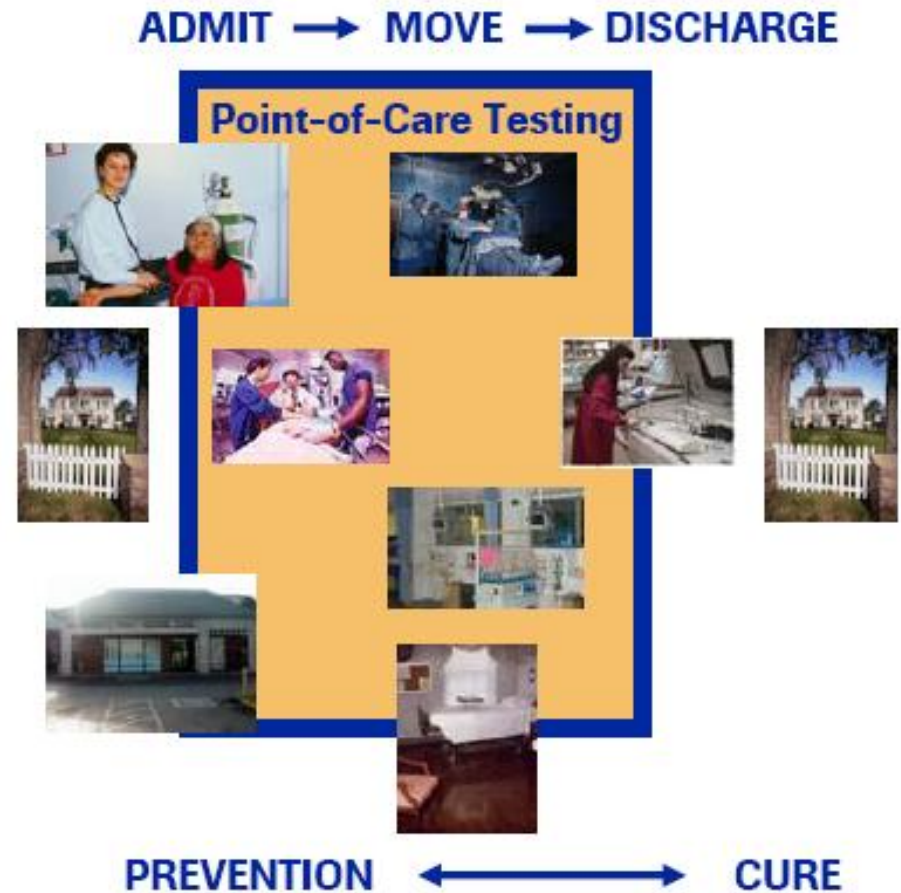
Ireland's EU Structural Funds
Programmes 2007 - 2013
Co-funded by the Irish Government
and the European Union



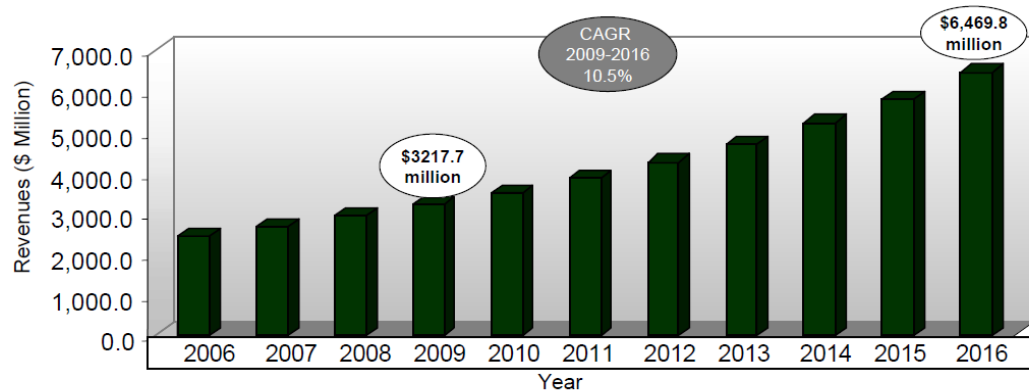
www.tyndall.ie/nanotech



- On-site testing
 - From the hospital to GP to home.
- Tests answering urgent questions:
 - Acute and chronic disease.
 - Rapid diagnosis
 - Therapeutic monitoring.
- Specific test needs
 - Fast & cheap
 - Simple to use
 - Reliable and reproducible results.
 - Simultaneous measurement
 - **Free from expensive Fluorescent Labels.**
- New markets opening up



Point of Care (POC) Biosensor Market: Revenue Forecasts (World), 2006-2016

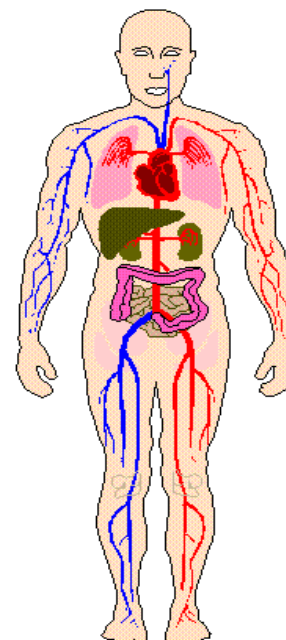


Note: All figures are rounded; the base year is 2009. Source: Frost & Sullivan

- Revenues in POC market expected to reach \$6.5b by 2016

POC market requirements:

- Convenient, easy to use and low maintenance requirements
 - Low cost (few cent – few dollars)
 - Provide rapid (<5 min), robust analysis
 - Detection limits same or better than clinical environment
 - Low power - disposable
- Nanosensor devices offer a potential solution to these needs**

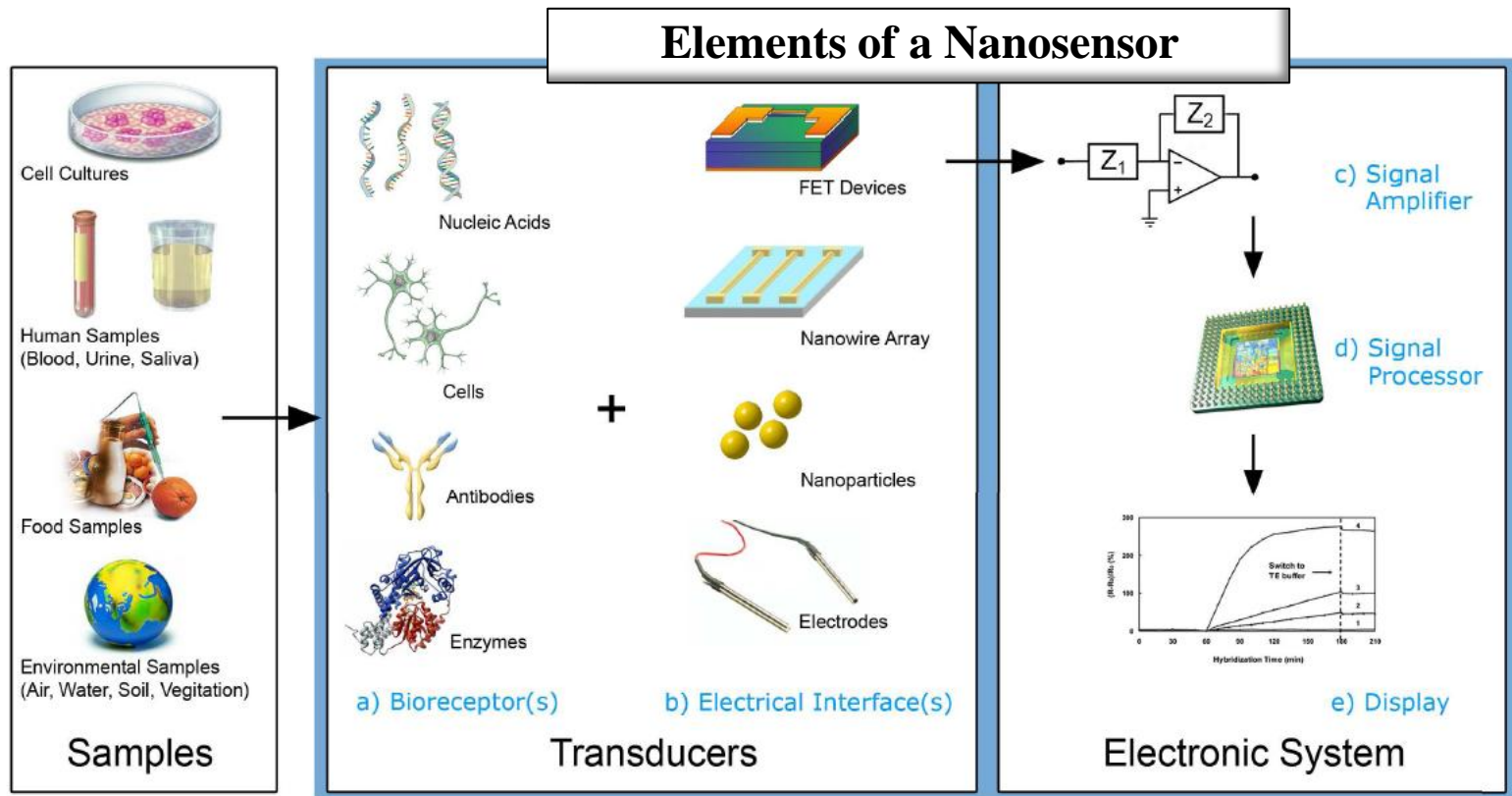


Abbott i-STAT portable clinical analyser

- Blood gases
- Electrolytes
- Hematology
- Coagulation
- Cardiac Markers



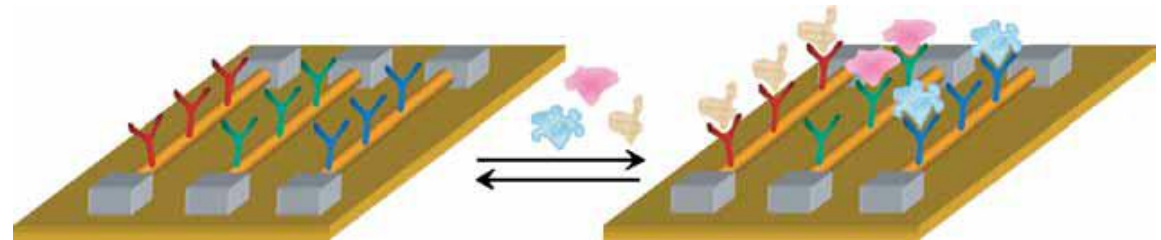
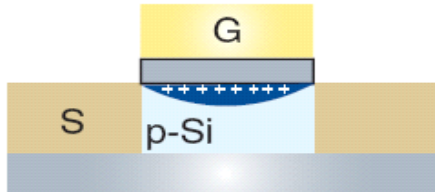
<http://www.abbottpointofcare.com>



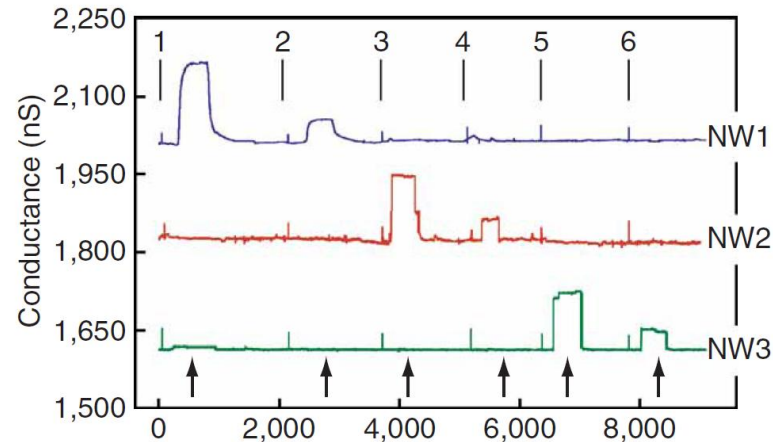
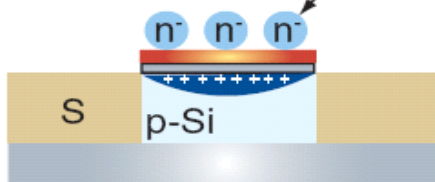
At the nanoscale:

- Sensor elements are of similar length scales to analytes
 - Lower limits of detection
 - Increased sensitivity & selectivity

Conventional FET



Molecular-Gated FET

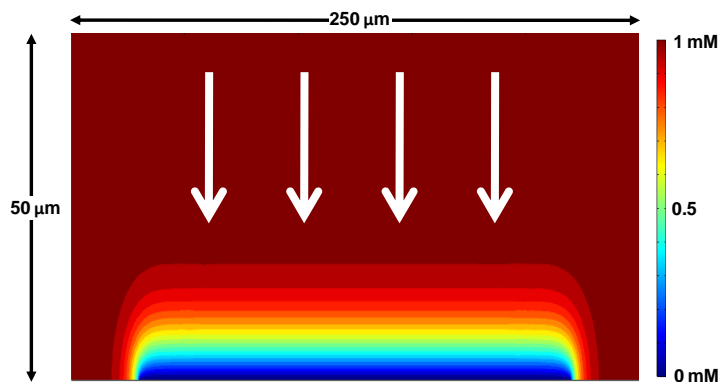


- **Dominant paradigm:** FET based sensing approaches (Si NW / CNTs).
- Highly sensitive detection of biomolecule including DNA, Viruses demonstrated (Vista Therapeutics).
- Complex fabrication approaches ➔ limited industrial take-up.
- Sometimes require for high back gate applied voltages (10 – 25 V).

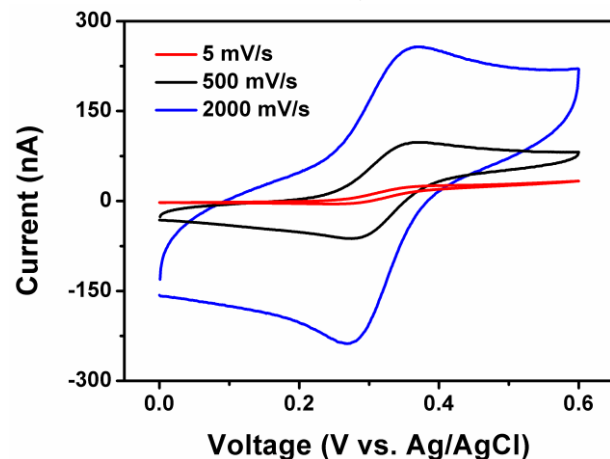
Lieber C. et al.

Nature Biotech. 23 (2005) 1294

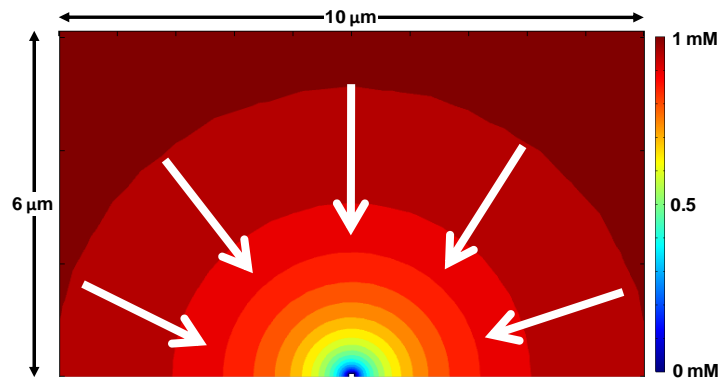
Planar Diffusion



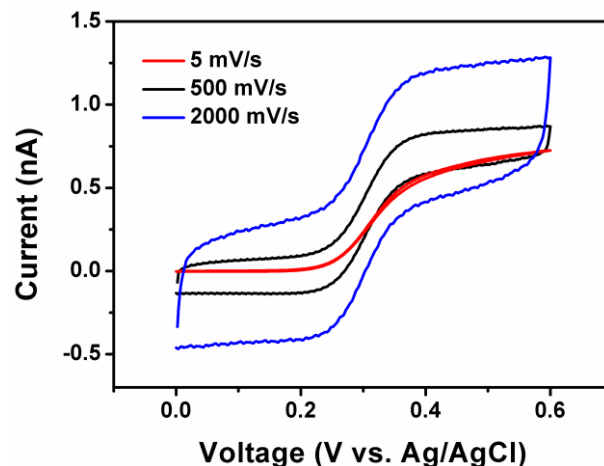
Micro-square Electrode:
 $w = 190 \mu\text{m}$



Radial Diffusion

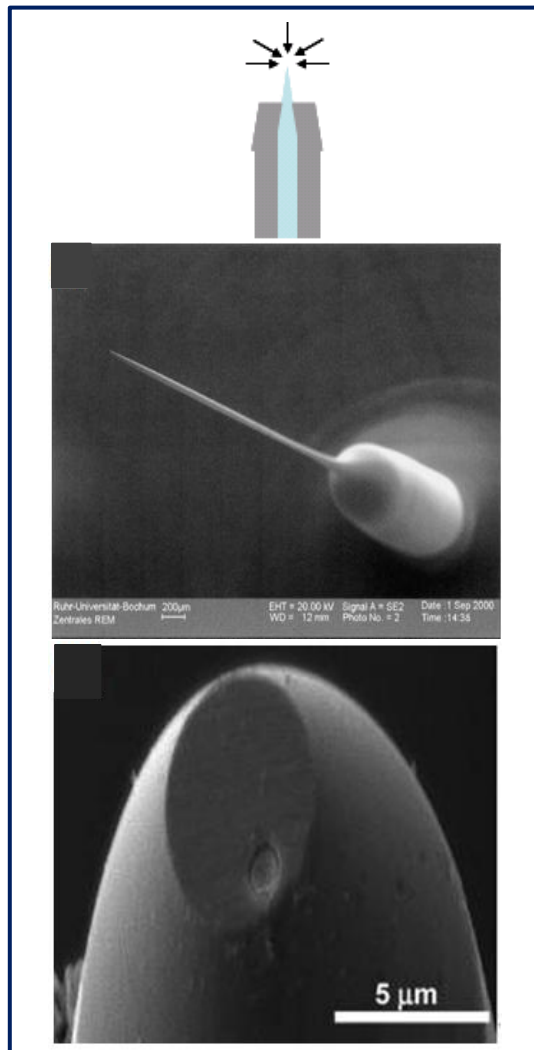


Single Nanowire:
 $w = 100 \text{ nm}, h = 50 \text{ nm}$

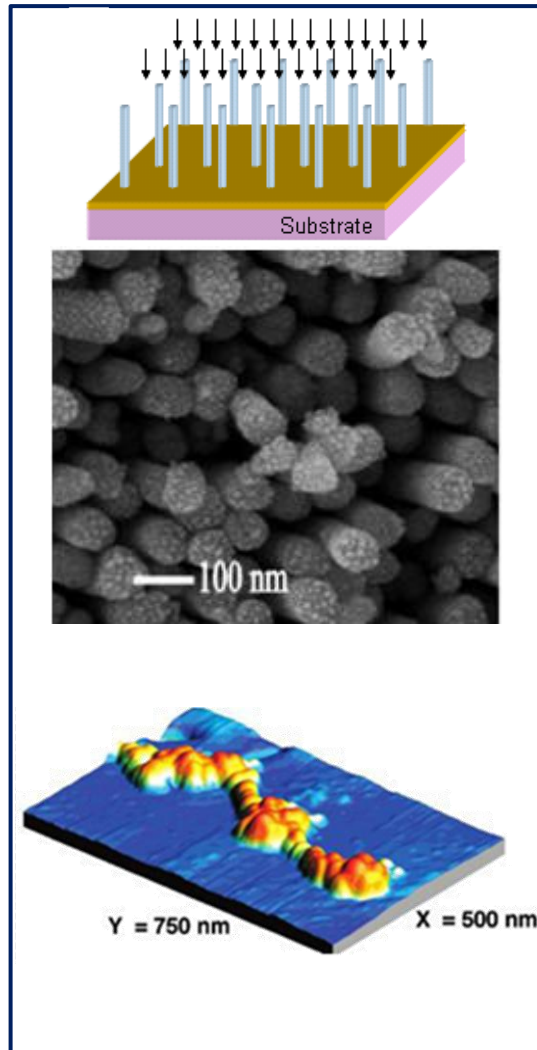


- At the nanoscale, radial analyte diffusion profiles dominate:
 - Increased in mass transport, improved current density → Higher S/N ratios
 - Steady-state measurements enable analysis at faster time intervals

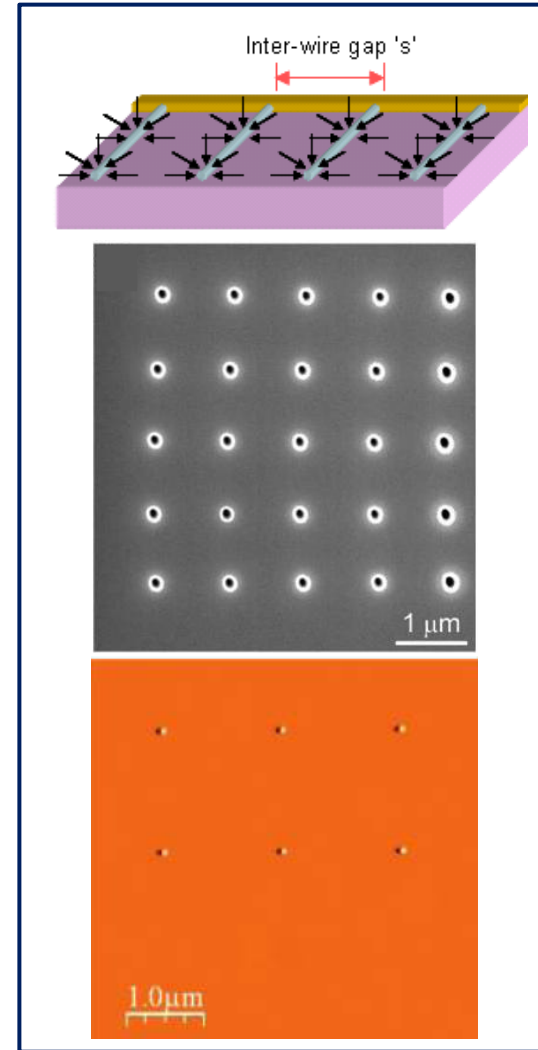
Single Nanoelectrodes



Nanoelectrode Ensembles



Nanoelectrode Arrays



Generation 1

- Single NW Electrode
- Bottom Up Approach
- Facile Integration
- In-depth Analysis
- Suitability to Sensing

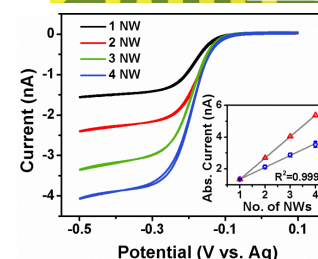
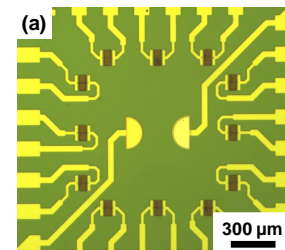
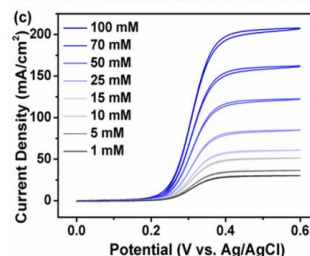
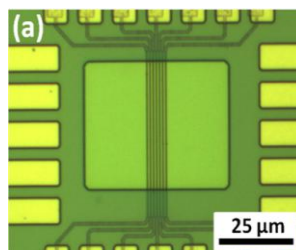
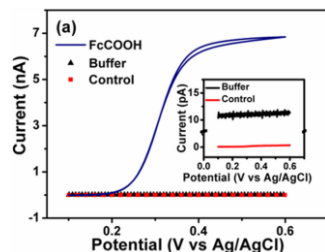
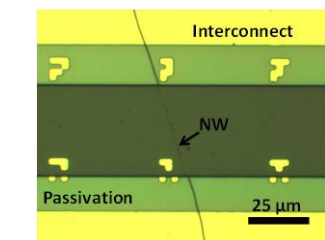
Generation 2

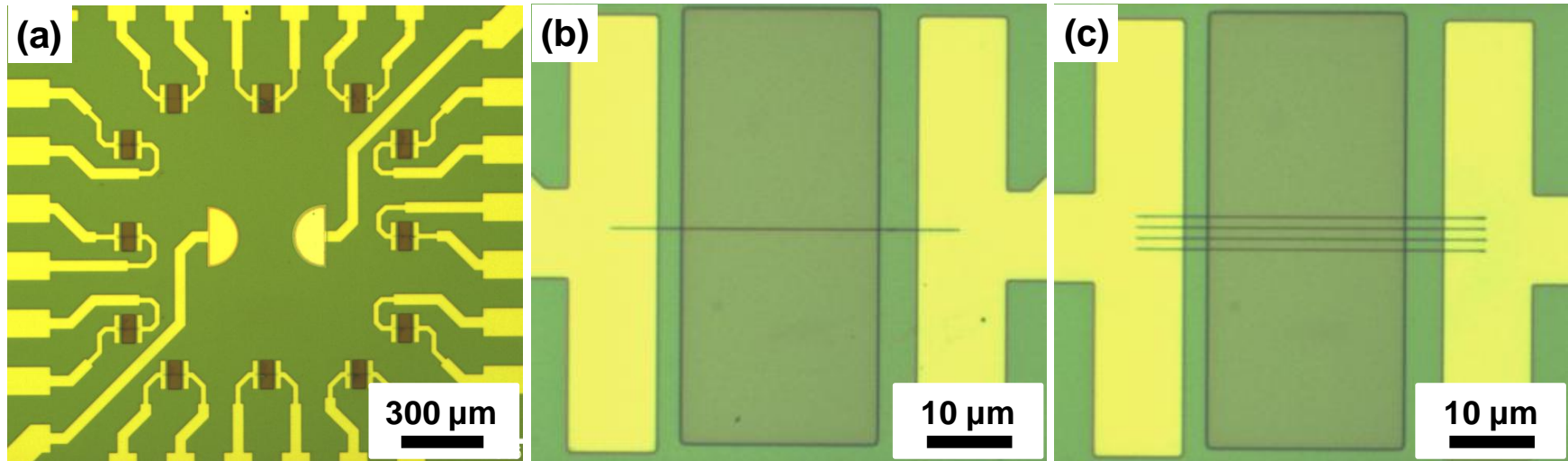
- Benchmark Gen 1
- Top Down Approach
- Reproducibility
- In-depth Analysis
- Glucose Detection

Generation 3

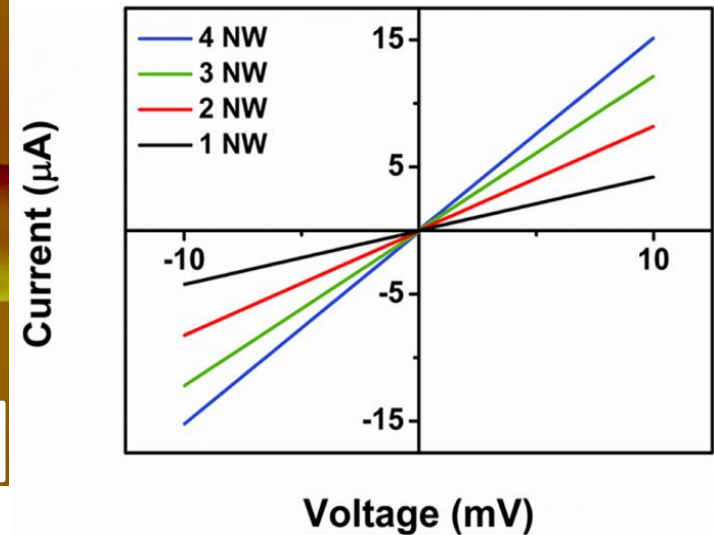
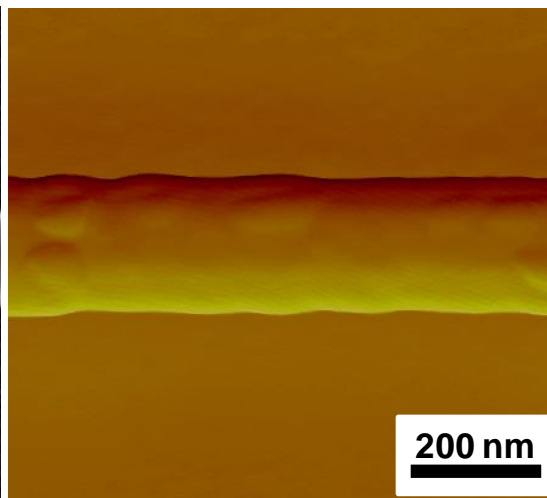
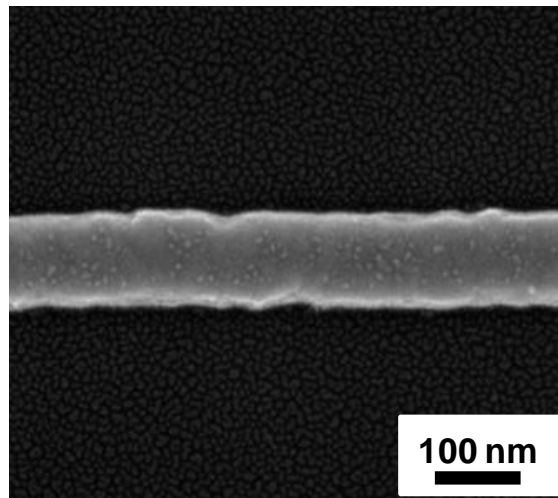
- Top Down Approach
- Platform Development
- Single NWs → Arrays
- Reduced packaging
- On-chip Counter Electrodes

Development of Nanowire Electrochemical Devices

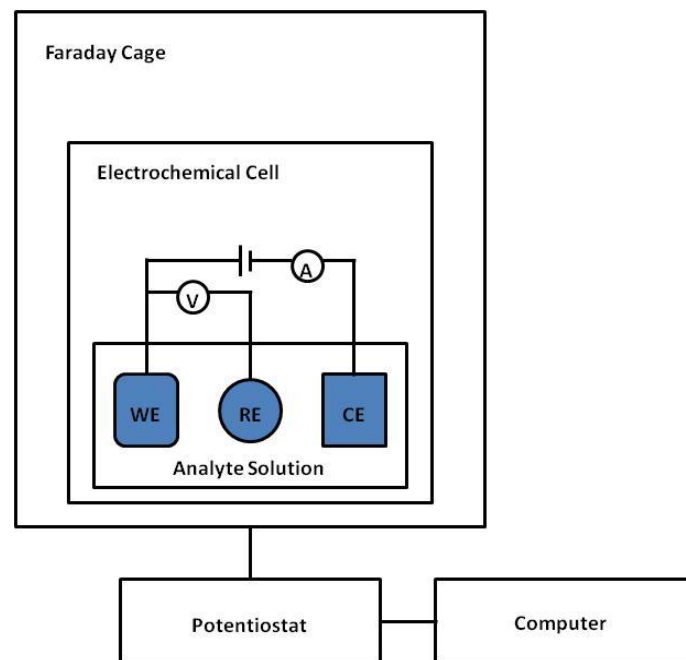
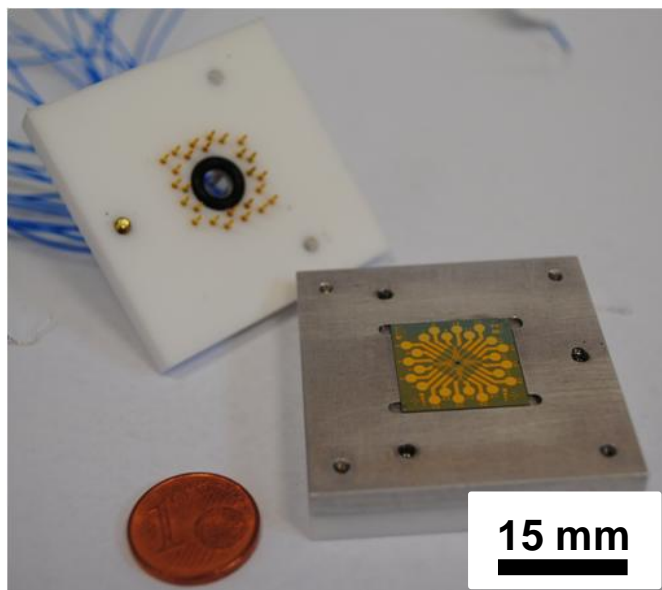




- Single nanowire electrodes and arrays of nanowire electrodes (2, 3 and 4 nanowires)
- Nanowire construction: 5 nm/50 nm Ti/Au
- Interelectrode distance in arrays $\sim 2 \mu\text{m}$
- On-chip Au counter electrodes located in the centre of device
- Silicon Nitride passivation layer $\sim 500 \text{ nm}$ thick



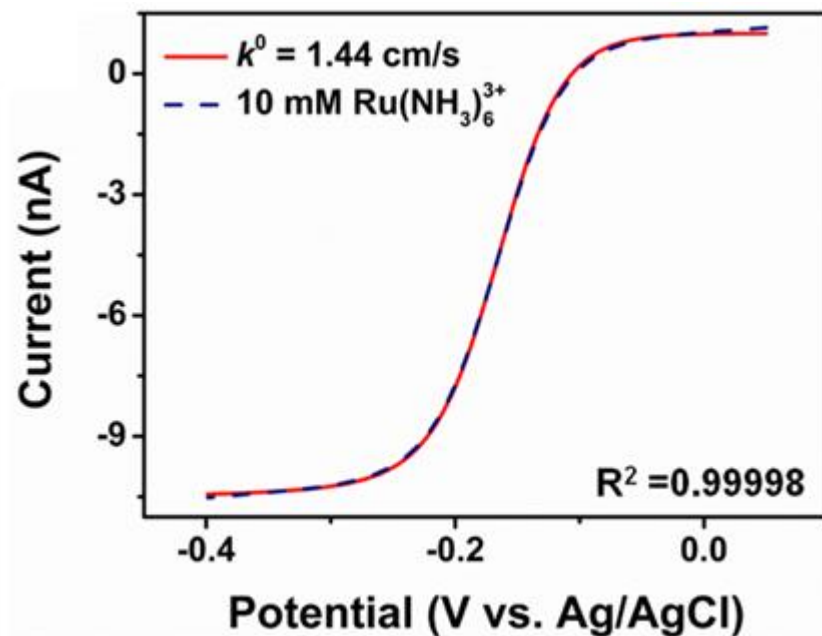
- Nanowire dimensions: width ~ 100 nm, height ~ 50 nm
- Nanowires and nanowire arrays displayed Ohmic electrical responses
- Increasing conductance was observed with increasing nanowires in array
- Average resistance for single nanowire was $\sim 2050 \pm 160 \Omega$
- Average resistance for array of 4 nanowires $\sim 360 \pm 160 \Omega$



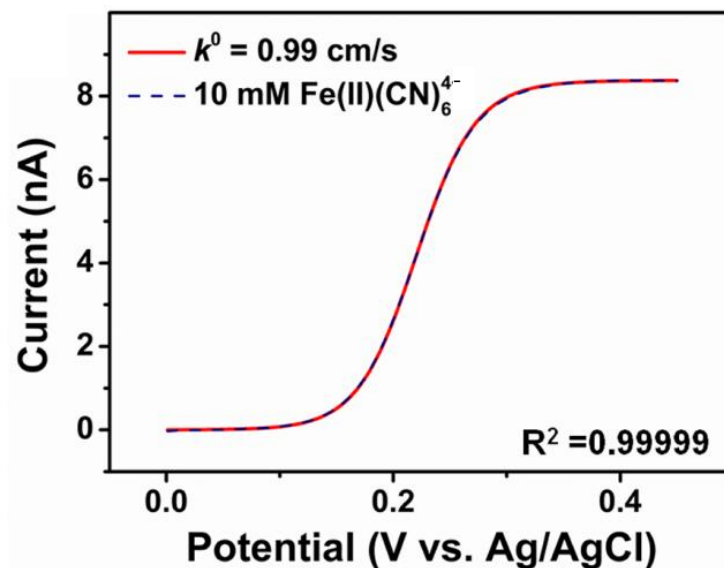
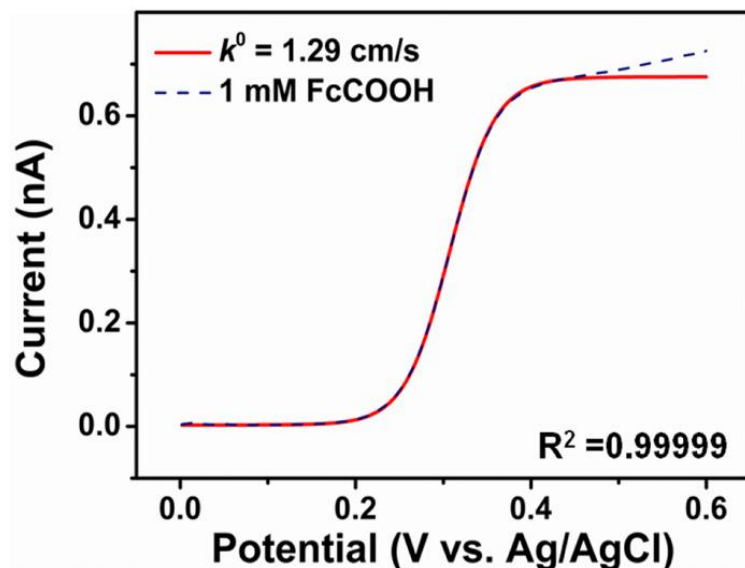
- Novel electrochemical cell removes packaging requirements
- Electrochemical cell volume $\sim 150 \mu\text{L}$
- Steady-state reductive voltammetric responses in $1 \text{ mM Ru}(\text{NH}_3)_6^{3+}$ in 10 mM PBS
- Average cathodic current at single nanowire: $-1.355 \pm 0.032 \text{ nA}$
- Low background current observed in buffer solutions only

$$k_{red} = k^0 e^{-\alpha F(E - E^{0'})/RT}$$

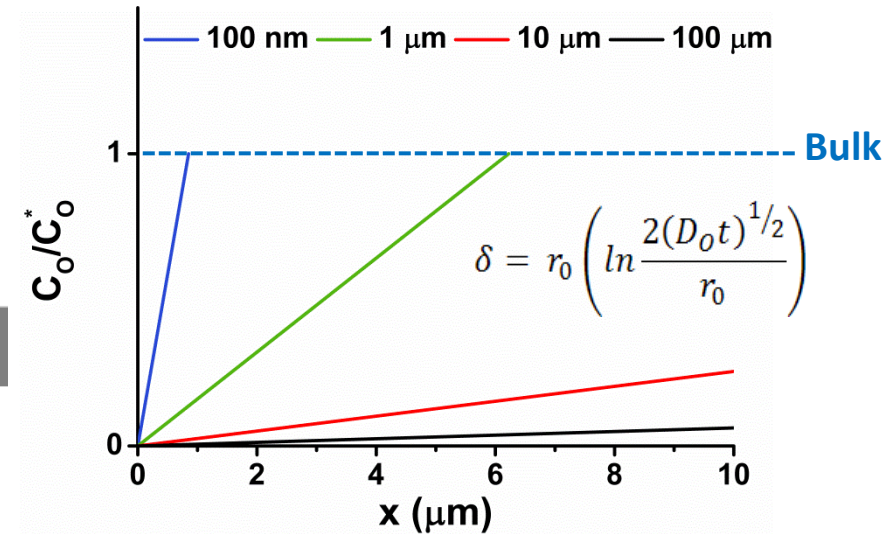
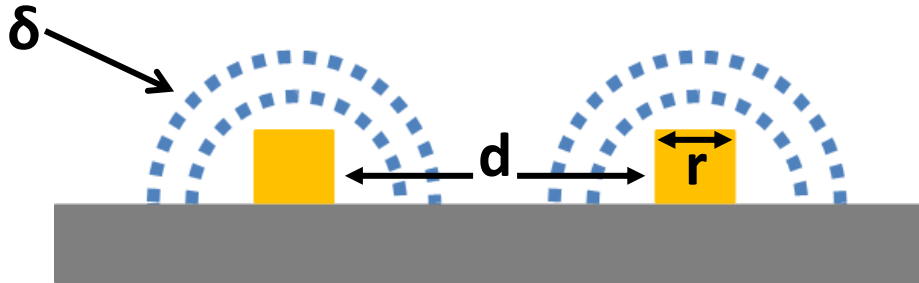
$$i_{bv} = \frac{i_{mt}}{1 + e \left[\frac{-F(E - E^{0'})}{RT} \right] + \frac{m}{k^0} e \left[\frac{\alpha F(E - E^{0'})}{RT} \right]}$$



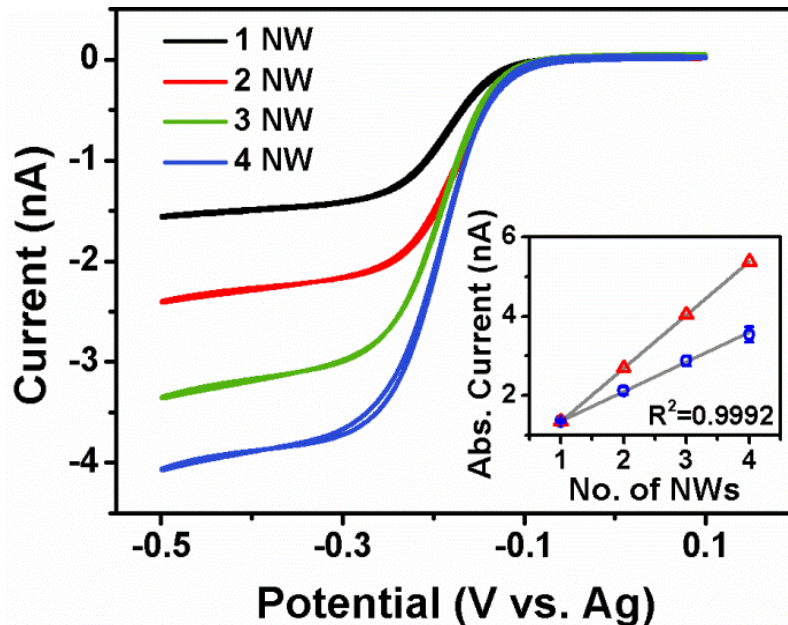
- Reduction of $\text{Ru(NH}_3)_6^{3+}$ at nanowire electrodes was found to be excellently described by Butler-Volmer kinetics
- An average k^0 value of 1.2 cm/s was determined
- Values consistent with those reported



- Single electron oxidation reactions of FcCOOH and $\text{Fe}(\text{CN})_6^{4-}$ excellently described by Butler-Volmer kinetics
- High k^0 values determined in both cases indicates rapid electron transfer to nanowires
- Values observed for FcCOOH consistent with values observed at nanoskived nanowires
- k^0 values for $\text{Fe}(\text{CN})_6^{4-}$ consistent with that reported for nanodisk electrode of radius $\sim 11 \text{ nm}$

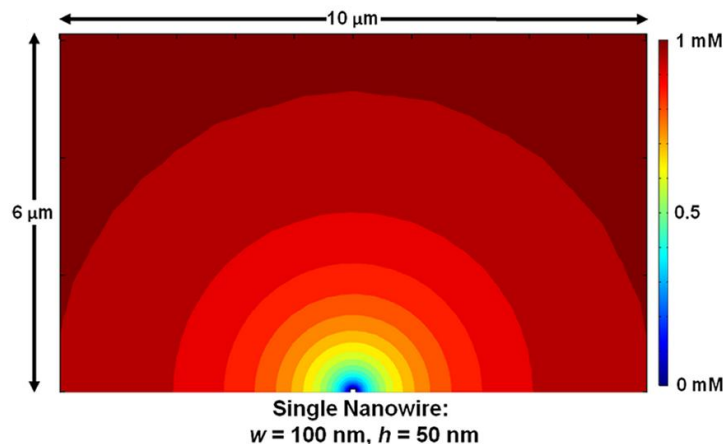
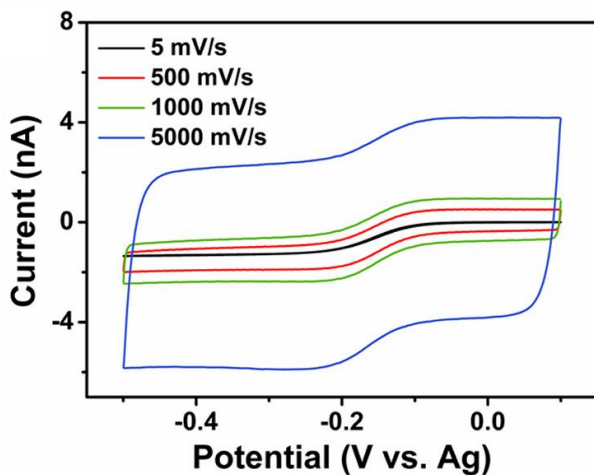


- Nernst diffusion layer is distance to bulk concentration from electrode.
- In arrays neighbouring diffusion profiles should not overlap.
- Estimated thickness of diffusion layer for single nanowire was ~ 850 nm for $r_0 = 100$ nm
- Nanowire Arrays designed with $2 \mu\text{m}$ spacing $\rightarrow d > 2\delta$

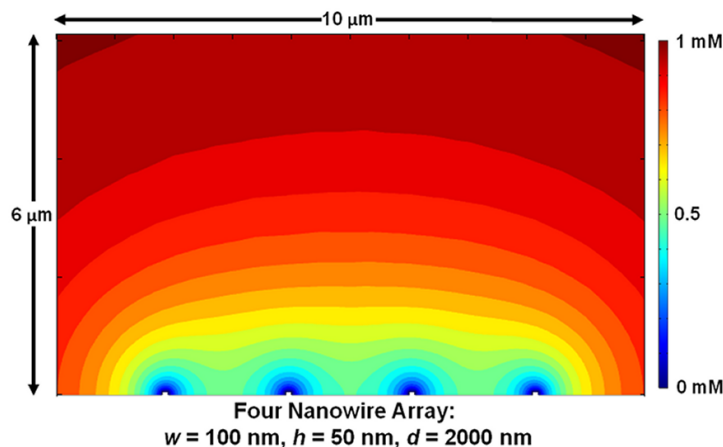
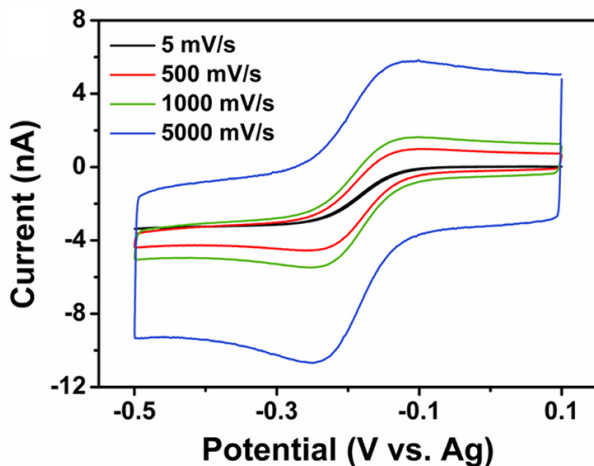


- Steady-state current was observed at all arrays.
- Increased current was measured with increasing nanowires in array.
- However measured current at 4 nanowires \neq 4 x 1 nanowire.
- Indicates that interelectrode spacing of $\sim 2 \mu\text{m}$ may not be sufficient to provide independent diffusion to each electrode in the array.

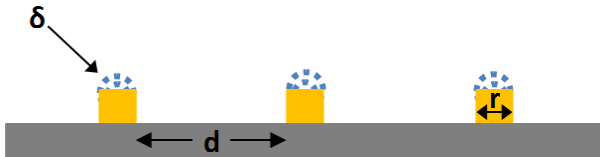
Single Nanowire Electrode



4 Nanowire Electrode Array



(i) $\delta \ll r \rightarrow$ Planar Diffusion



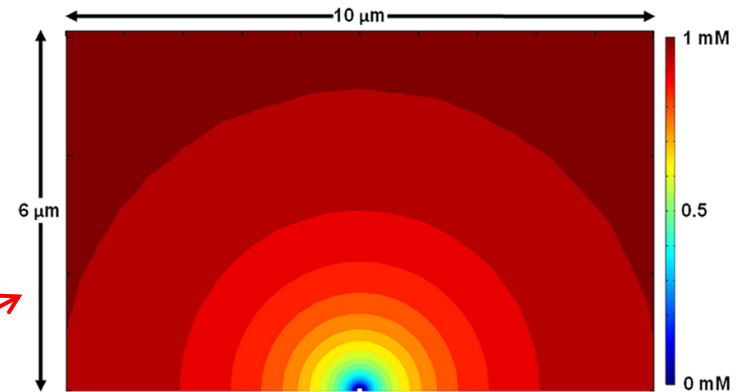
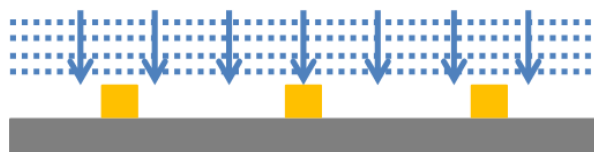
(ii) $\delta = r < d \rightarrow$ Radial Diffusion



(iii) $r < \delta \leq d \rightarrow$ Transition Zone



(iv) $\delta \gg d \rightarrow$ Planar Diffusion

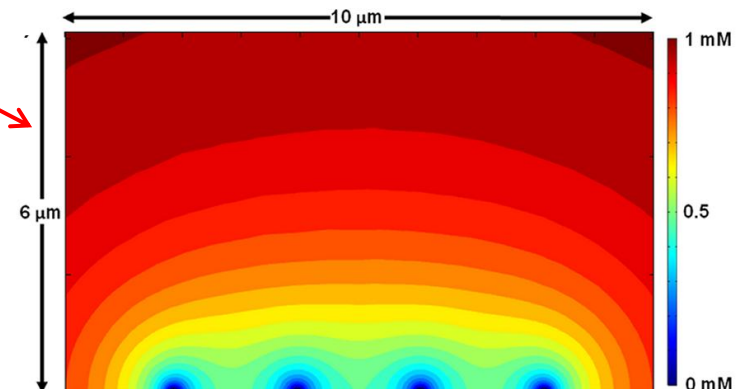


Single Nanowire:
 $w = 100 \text{ nm}$, $h = 50 \text{ nm}$

δ = diffusion layer thickness

r = critical dimension

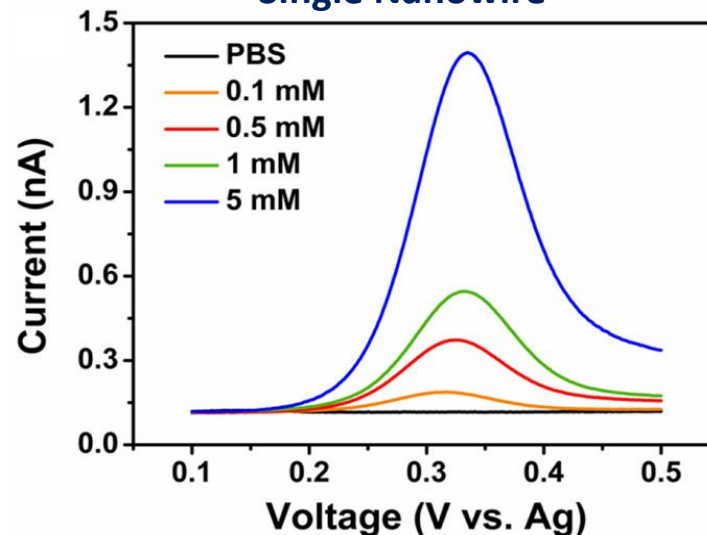
d = interelectrode distance



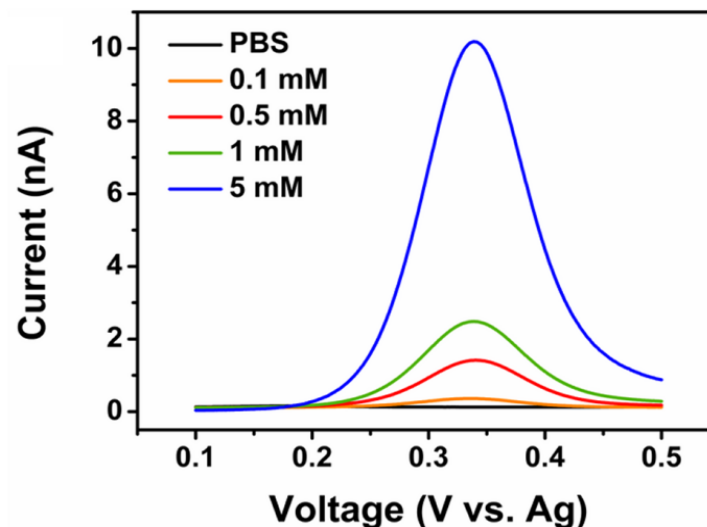
Four Nanowire Array:
 $w = 100 \text{ nm}$, $h = 50 \text{ nm}$, $d = 2000 \text{ nm}$

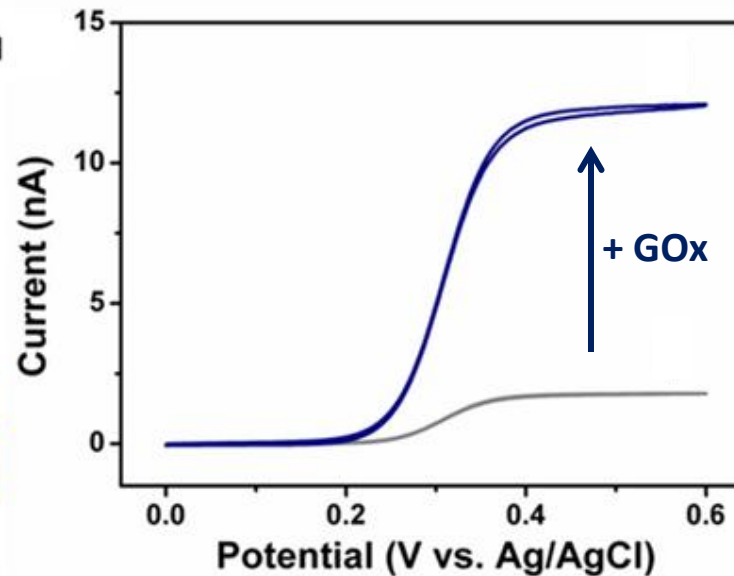
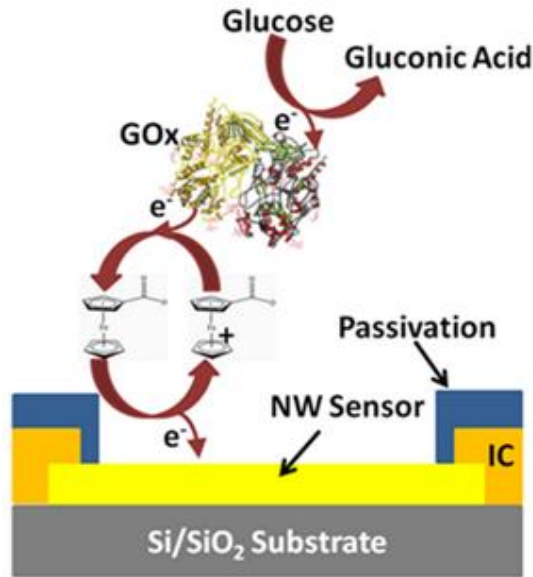
- Square Wave Voltammetry is commonly used electroanalytical technique
 - Increased Faradic signal
 - Reduced Capacitive signal
 - Higher S/N
 - Lower detection limits
- SWV in range of concentrations of FcCOOH in 10 mM PBS
- Peak current for **single nanowire in 5 mM** ~ 1.4 nA
- Peak current for **4 NW Array in 5 mM** ~ 10.2 nA
- Peak current at **4 NW Array** > than 4 x 1 NW
- Demonstrates suitability of arrays towards sensing

Single Nanowire

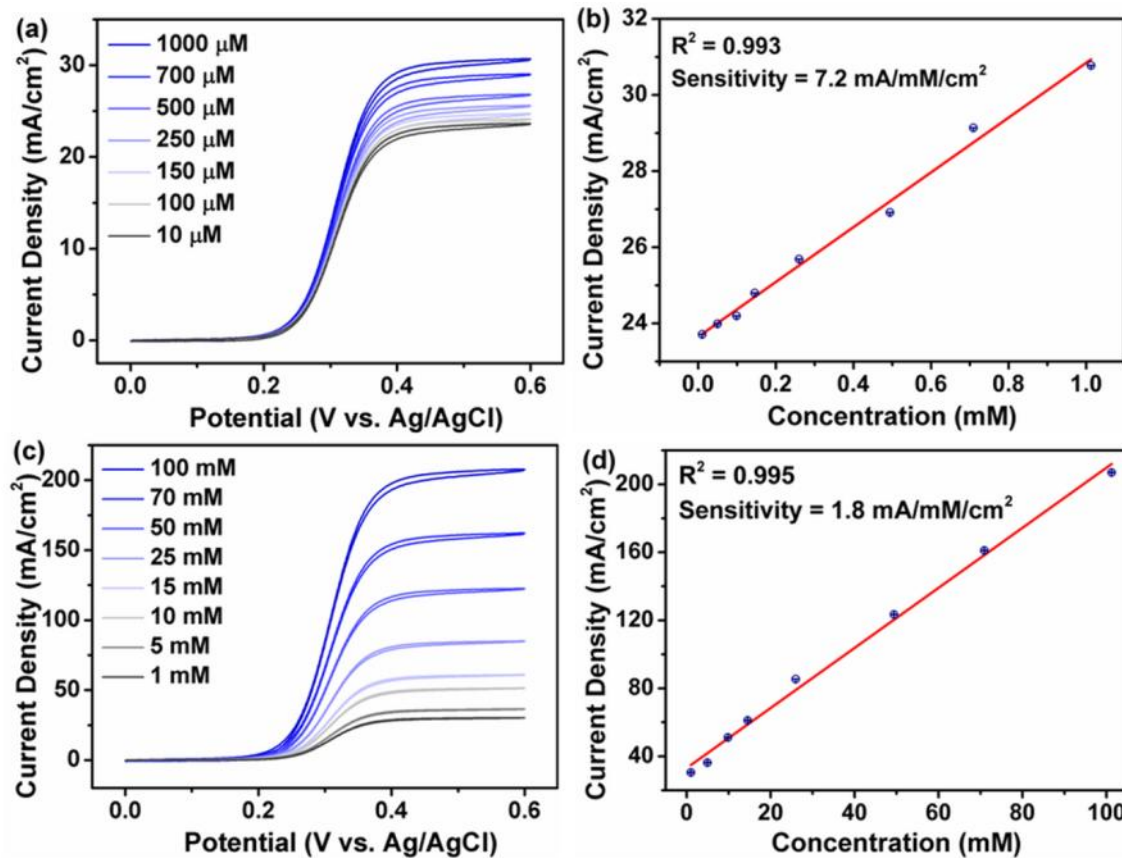


4 Nanowire Array





- Enzymatic detection of Glucose via Glucose Oxidase in the presence of a mediator, FcCOOH
- Redox Mediated detection:
 - Increases measureable signal
 - Reduces overpotentials required to oxidise Glucose
 - Reduces contributions from interfering species
- In absence of GOx, only FcCOOH signal measured in the presence of Glucose



- Measurement range : 10 μM – 100 mM Glucose

Lower linear range 10 μM –1 mM:

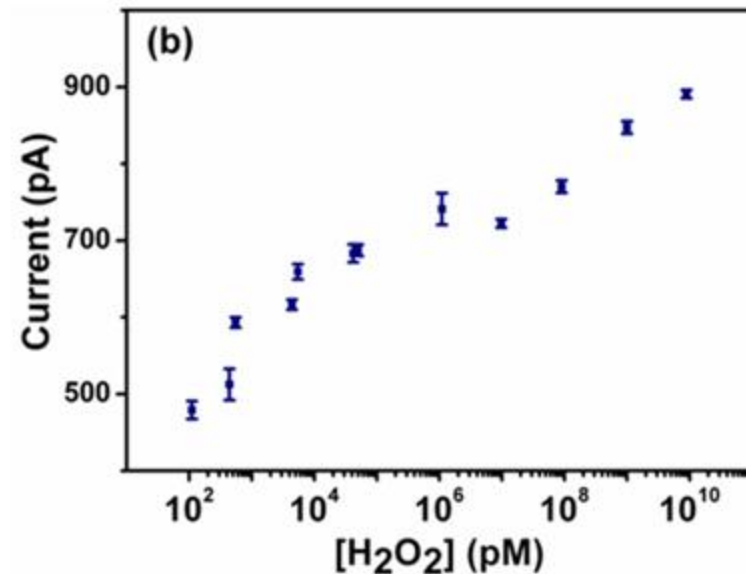
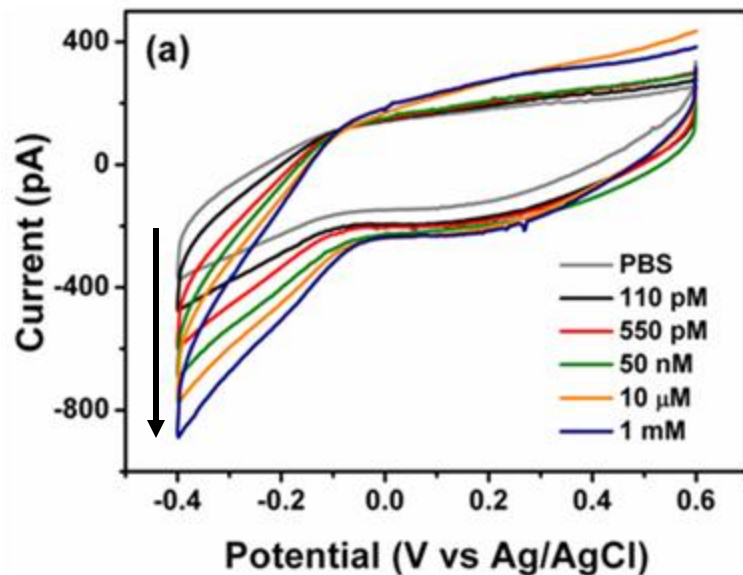
- LOD $\sim 3 \mu\text{M}$
- High sensitivity $\sim 7.2 \text{ mA}/\text{mM}/\text{cm}^2$

Upper linear range (1 mM–100 mM):

- LOD: $\sim 17 \mu\text{M}$
- Sensitivity $\sim 1.8 \text{ mA}/\text{mM}/\text{cm}^2$
- Nano-SOA: $\sim 0.005 \text{ mA}/\text{mM}/\text{cm}^2$

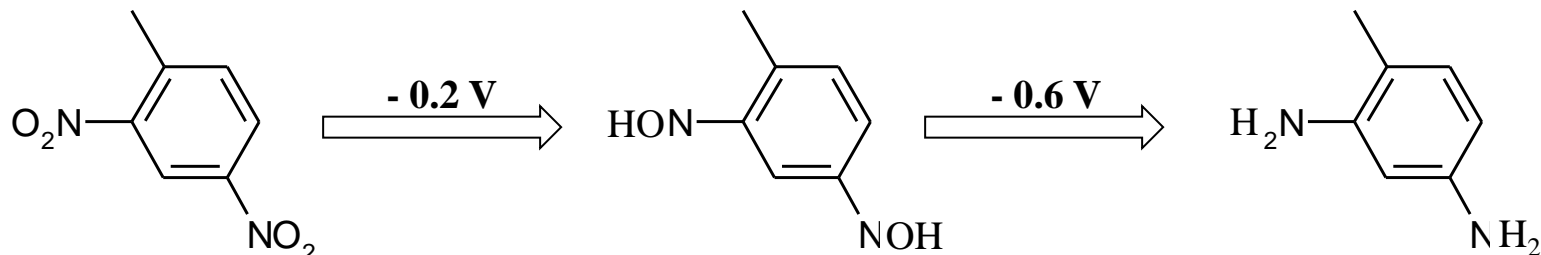
- Blood glucose required detection range: 0.5 mM – 15 mM
- Alternative media e.g. saliva or tears: $\sim 100 \mu\text{M}$ – 500 μM

K. Dawson, et al, *Analyst*, **2011**, 136 (21), 4507-4513.



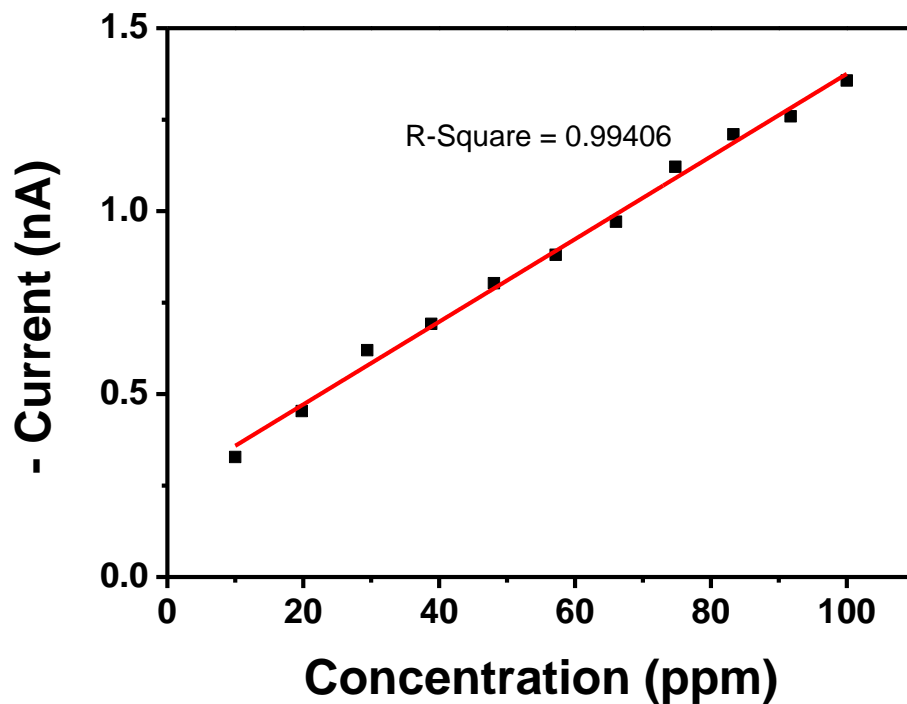
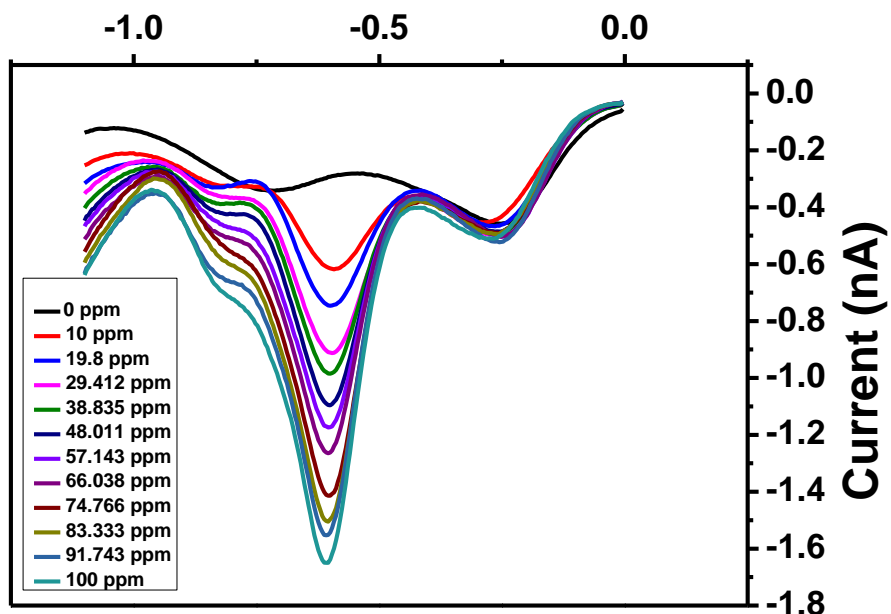
- H_2O_2 key target analyte: environmental analysis, food spoilage, biomedical applications & homeland security
- Requires low detection limits over wide concentration range
- CV of H_2O_2 exhibits a reductive peak at -0.4 V vs. Ag/AgCl in 100 mM PBS, pH 7.0
- Detection range 10^{-10} to 10^{-2} M, lowest concentration detected 110 pM
- Comparative to detection limits observed for modified electrodes (Prussian blue, HRP)

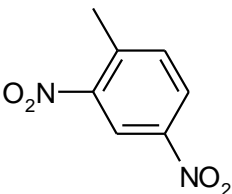
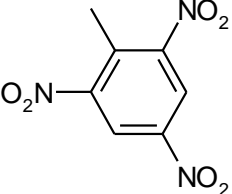
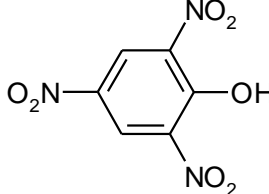
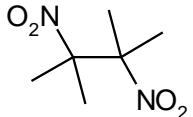
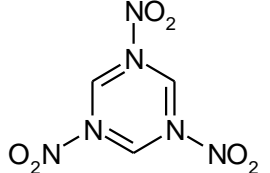
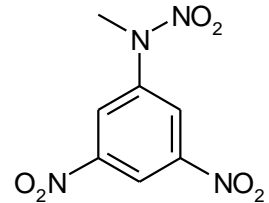
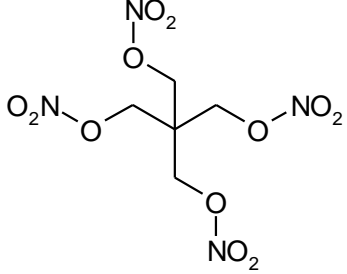
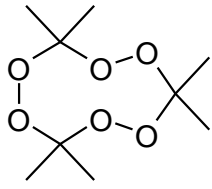
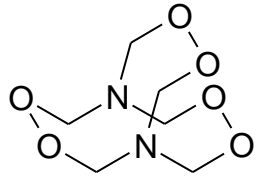
K. Dawson, et al *Anal. Chem.*, 2011, 83, 5535-5540.



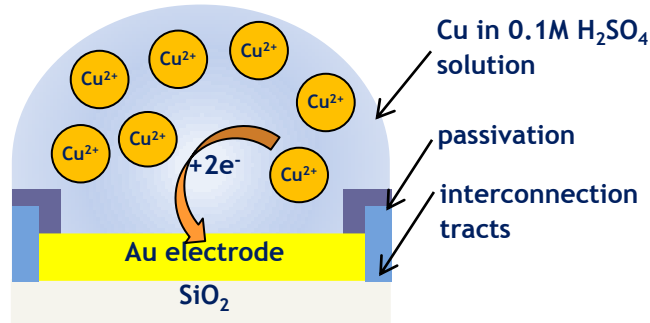
2,4-Dinitrotoluene (DNT)

Voltage (V)

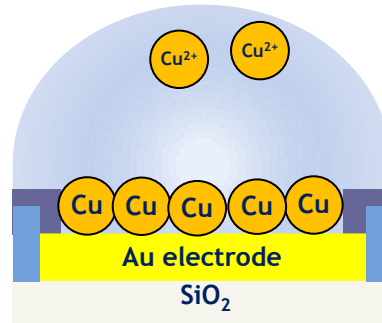


 <p>2,4-Dinitrotoluene (DNT)</p>	 <p>2,4,6-Trinitrotoluene (TNT)</p>	 <p>Picric acid (PA)</p>
 <p>2,3-Dimethyl-2,3-dinitrobutane (DMNB)</p>	 <p>Cyclotrimethylenetrinitramine (RDX)</p>	 <p>2,4,6-Trinitrophenyl-N-methylnitramine (Tetryl)</p>
 <p>Pentaerythritol tetranitrate (PETN)</p>	 <p>Triacetone triperoxide (TATP)</p>	 <p>Hexamethylene triperoxide diamine (HMTD)</p>

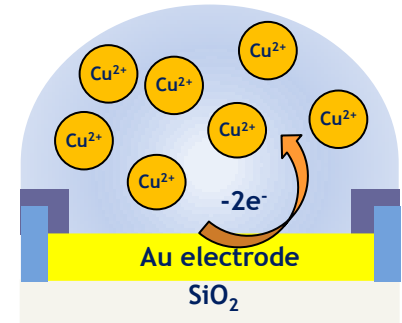
Molecular structure of common explosive compounds



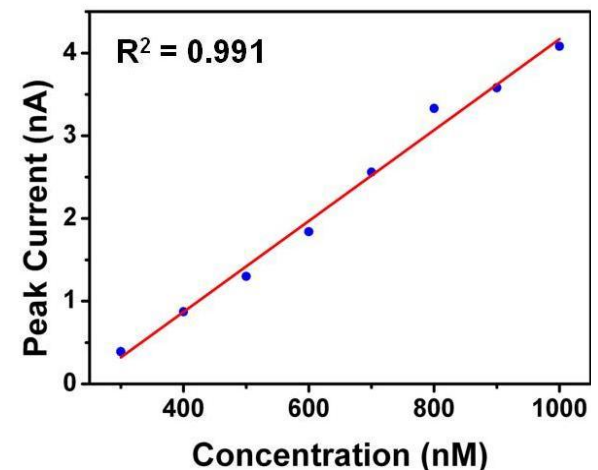
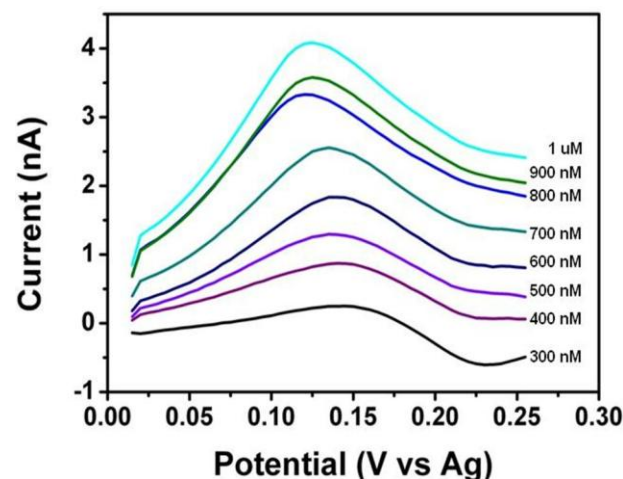
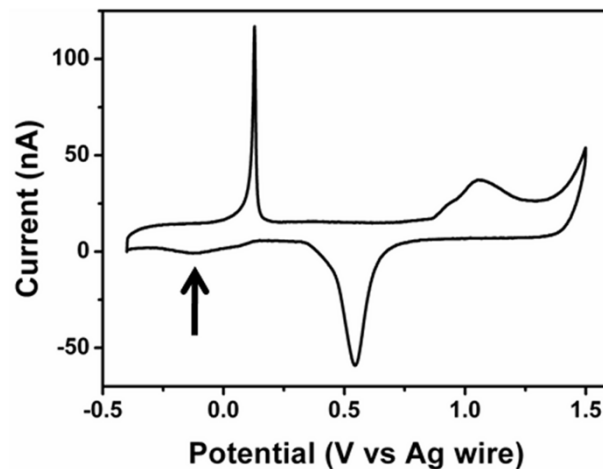
1. UPD: $E = 0.0 \text{ V}$ (vs Ag/AgCl) and $t = 0, 30, 60 \dots \text{X s}$



2. Deposition of a monolayer of Cu onto the gold surface of the electrode




3. SV to remove the Cu from the electrode surface



–(a) Background subtracted stripping voltammograms of a series of Cu^{2+} solutions in $0.1\text{M H}_2\text{SO}_4$ at a gold nanowire electrode for 60s. (b) Electrochemical current vs. concentration for a deposition time of 60s.

- Single nanowire electrodes exhibited steady state – behaviour, fast electron transfer kinetics and low capacitance.
- Increased detection limits for Hydrogen Peroxide at unmodified electrodes
- Enhanced sensitivity to Glucose detection at nanoelectrodes – detection in non-capillary media (pain free)
- Applied to the detection of cations and organic molecules
- Diffusion controlled – design for use

 <p>SEVENTH FRAMEWORK PROGRAMME</p>	Phast-ID	FP7-ICT-2009 (STREP)
	CommonSense	FP7-SEC-2010-1 (STREP)
	E-Brains	FP7-ICT-2009-5 (STREP)
	NanoFunction	FP7-ICT-2009-5 (NOE)

 <p>science foundation ireland fondúireacht eolaíochta éireann</p>
SFI/ 09/RFP/CAP2455 (RFP)



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www.tyndall.ie/nanotech



UCC

Coláiste na hOllscoile Coraigh, Éire
University College Cork, Ireland

Generation 1

- Single NW Electrode
- Bottom Up Approach
- Facile Integration
- In-depth Analysis
- Suitability to Sensing

Generation 2

- Benchmark Gen 1
- Top Down Approach
- Reproducibility
- In-depth Analysis
- Glucose Detection

Generation 3

- Top Down Approach
- Platform Development
- Single NWs → Arrays
- Reduced packaging
- On-chip Counter Electrodes

Development of Nanowire Electrochemical Devices

